

Eulerian formulation of inelasticity – from metal plasticity to growth of
biological tissues

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Abstract

The Lagrangian formulation of metal plasticity by Bilby et al. (1957), Kroner (1959) and Lee (1969) is based on the total deformation gradient \mathbf{F} from a fixed reference configuration and a plastic deformation measure \mathbf{F}_p from the reference configuration to a stress-free intermediate configuration. The elastic deformation can be defined by $\mathbf{F}_e = \mathbf{F}\mathbf{F}_p^{-1}$. Besseling (1966) proposed an evolution equation for \mathbf{F}_e . Eckart (1948) proposed an Eulerian evolution equation directly for an elastic deformation measure to model elastically isotropic elastic-inelastic material response. Leonov (1976) developed the same theory for polymeric liquids. Motivated by this work, Rubin (1994) proposed Eulerian evolution equations for a triad \mathbf{m}_i of microstructural vectors that model elastic deformation for fully anisotropic elastic-inelastic response. In contrast with the Lagrangian formulation, this Eulerian formulation is insensitive to arbitrariness of the choices of: a reference configuration, an intermediate configuration, a total deformation measure and a plastic deformation measure. For elastically isotropic response, Eulerian evolution equations are proposed for the elastic dilatation J_e and a unimodular elastic distortional deformation tensor \mathbf{B}'_e . For growth of biological tissues, the evolution equations have been modified to model homeostasis, which is the inelastic process that causes a tendency for J_e, \mathbf{B}'_e to approach their homeostatic values J_h, \mathbf{H}' . In particular, the stress in the homeostatic state can be non-zero. Constitutive equations must be proposed for both the homeostatic values J_h, \mathbf{H}' and the rates Γ_m, Γ of dilatational and distortional homeostasis, respectively. Robust, strongly objective numerical algorithms will also be discussed.